

## Interpretation of the Inotropic Effect of 2,3-Butanedione Monoxime on the Isometric Twitch of Guinea-pig Papillary Muscle

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**Abstract.** The negative inotropic effect of 2,3-butanedione monoxime (BDM) on the isometric twitch of guinea-pig papillary muscle was analysed by parameters characterizing the time course of the mechanogram. BDM at concentrations of up to 4 mmol/l produced a clear negative inotropic effect, whereas the Ca transient measured in isolated cardiomyocytes was only slightly affected. Peak force was more reduced than  $dF/dt_{\max}$  and  $dF/dt_{\min}$ . This led to an earlier, more narrow peak and a shortening of twitch duration. Based on a reaction scheme for the cross-bridge cycle, a mathematical model using a Ca transient and mechanograms as input data has been developed. The kinetic parameters were estimated by fitting the model to various time courses of force obtained at rising concentrations of BDM. BDM decreased the ratio of rate constants for cross-bridge attachment and detachment in a concentration-dependent manner: the formation of cross-bridges became inhibited, whereas dissociation was promoted. Above 4 mmol/l BDM the more marked alterations of the parameters of the mechanogram indicated an additional suppressing effect on intracellular Ca supply. The computer analysis suggests how the cellular mechanism(s) of the BDM-induced negative inotropic effect are reflected in the time course of the mechanogram.

**Key words:** 2,3-Butanedione monoxime — Ca transient — Isometric contraction — Mathematical model — Guinea-pig papillary muscle

## Introduction

Force development of the myocardium is determined by inotropic mechanisms influencing the release and the removal of intracellular Ca ( $\text{Ca}_i$ ) and the sensitivity of the myofilaments for Ca. The time course of force is modified in a characteristic manner, i.e. different inotropic mechanisms show a characteristic pattern of parameters of the mechanogram (Bogdanov et al. 1979; Honoré et al. 1987; Gross et al. 1989). A computer programme was developed to estimate parameters for contraction and relaxation which can be used to characterize inotropic effects on isolated cardiac preparations (Lammerich 1992).

The intracellular Ca transient results from processes regulating the Ca homeostasis. Inotropic effects with an only modest modification of  $\text{Ca}_i$  supply should have affected the utilization of  $\text{Ca}_i$  by the myofilaments. Fulfilling this, the negative inotropic effect of low BDM concentration on the myocardium of several species (Blanchard et al. 1990; Perreault et al. 1992; Spurgeon et al. 1992; Steele and Smith 1993; Kotsanas et al. 1993; Backx et al. 1994) and on that of the guinea-pig (Marijic et al. 1991; Gambassi et al. 1993) is not attributed to insufficient  $\text{Ca}_i$  supply (but cf. Gwathmey et al. 1991). We measured nearly unchanged Ca transients in guinea-pig cardiomyocytes at low BDM concentration. As a consequence, alterations in Ca sensitivity of the myofilaments have to be expected. This should be recognizable by a detailed analysis of the mechanogram. In order to interpret the changes in the time course of a twitch appearing at low concentrations of BDM, a reaction scheme was employed including the main steps of force development within the sarcomere (Yue 1987) instead of more complicated and complex approaches (Backx et al. 1994; Zhao and Kawai 1994). A mathematical model using a Ca transient and mechanograms as input data has been developed to calculate the rate constants for cross-bridge attachment and detachment as the essential determinants for the alteration of force development due to BDM.

## Materials and Methods

The experiments were performed on 10 guinea-pig right ventricular papillary muscles. The bathing solution, oxygenated with pure  $\text{O}_2$  at  $31^\circ\text{C}$ , had the following composition (in mmol/l): NaCl 140, KCl 5.4,  $\text{CaCl}_2$  0.5,  $\text{MgCl}_2$  1.1, Tris-HCl 10.0, glucose 11.1 at pH 7.43.

Electrical stimulation and measurement of isometric force  $F$  at a preload of 2 mN were performed using the programmable stimulator module PSM 676 and the force transducer F10 connected to the bridge amplifier DBA 660 of the Plugsys system 603 (Hugo Sachs Elektronik, Germany). The analogue force signal was digitized and stored by a personal computer. The preparations were stimulated with biphasic rectangular impulses of 10 ms duration and a strength of 30% above threshold.

At a stimulation frequency of 0.25 Hz, peak force ( $PF$ ) became stable after about 25 min. During the subsequent experiment at a stimulation frequency of 0.5 Hz, extra-

cellular Ca was elevated up to 18 mmol/l by adding  $\text{CaCl}_2$  stock solution in order to reach maximum  $PF$  as starting-point for the expected negative inotropic effect of BDM (purchased from Sigma). [BDM] was gradually increased as seen in the results.

Osmolarity was not compensated after the addition of Ca, because only extreme changes of intracellular volume and of ionic strength are known to influence the cross-bridge cycling (Allen and Smith 1987). Therefore, high extracellular Ca concentration is frequently used without compensation of osmolarity (e.g. Gwathmey et al.; Marijic et al. 1991) to avoid other consequences of disturbed distribution of physiologically important ionic concentrations.

Furthermore, these control conditions remain constant throughout the whole following protocol. BDM is likely to be distributed uniformly in the intra- and extracellular fluid, therefore its effects should not be modified by a shift of water.

Isolated cardiomyocytes were prepared by enzymatic dissociation according to Lewartowski et al. (1994). For the measurement of Ca transients cells were loaded with indo-1-ester (Lewartowski et al. 1994). Indo-1 Ca transients were monitored as a ratio 405/495 during rhythmical field stimulation.

### Software

The software in Turbo Pascal developed in our laboratory (Lammerich 1992) includes control of the experimental setup and data acquisition, the analysis of the mechanogram and statistics. A programme for control of the experiment and data acquisition permits stimulation with any chosen stimulus by the Plugsys module PSM 676. The registration of force for a desired number of twitches is synchronously started with the stimulus. The experimental protocol can be preselected. Support for calibration and adjustment of the base line is available. Values of  $PF$  and contraction curves are shown on the screen, condensed and stored. All information concerning the experimental procedure is saved in a protocol file allowing a fast survey of the experiment.

### Analysis

The following parameters for contraction and relaxation were estimated from the filtered and averaged data by the analysis programme:

$PF$  - peak isometric force;  $dF/dt_{\max}$  - maximum  $dF/dt$ ;  $dF/dt_{\min}$  - minimum  $dF/dt$ ;  $TL$  - time of latency;  $T50$  - time to 50% of  $PF$ ;  $TPF$  - time to peak force;  $RT50$  and  $RT97$  - relaxation time for the decline of force by 50% and 97% of  $PF$ , respectively;  $T(dF/dt_{\max})$  - time at  $dF/dt_{\max}$ ;  $(dF/dt_{\max})/PF$ ;  $(dF/dt_{\min})/PF$ ;  $(dF/dt_{\max})/(dF/dt_{\min})$ ;  $(dF/dt_{\max})/F$ ,  $(dF/dt_{\min})/F$  - quotient by  $dF/dt_{\max}$  and  $dF/dt_{\min}$ , respectively, and the corresponding instantaneous force;  $CPC$  - coefficient for the phasic component of the contraction, being the quotient of maximum and mean rate of force development:  $CPC = (dF/dt_{\max}) \cdot (TPF - TL)/PF$ ;  $CPR$  - coefficient for the phasic component of the relaxation, being the quotient of maximum and mean rate of force decline:  $CPR = (dF/dt_{\min}) \cdot RT97/PF$ .

The 0.1% level of  $PF$  served as the onset of force development at  $TL$ .

The  $dF/dt$  signal was calculated by a tested algorithm (Lammerich 1992) resulting in errors of about 1%. The  $dF/dt$  signal yielded  $dF/dt_{\max}$ ,  $dF/dt_{\min}$ ,  $T(dF/dt_{\max})$  and  $T(dF/dt_{\min})$ .

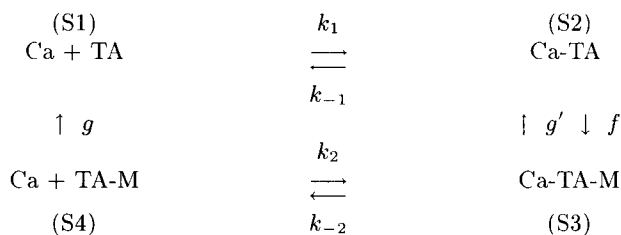
The appearance of an early phasic and late tonic component during the isometric contraction was assumed to arise from Ca, being delivered from different sources during

activation (Bogdanov et al. 1979; Honoré et al. 1987). The relation between  $dF/dt_{\max}$ , representing the phasic component, and the mean rate of force development, representing both phasic and tonic components, was expressed as the coefficient of the phasic components of the contraction (*CPC*). The phasic behaviour of the relaxation, expressed by *CPR*, was determined by various interactions of mechanisms leading to detachment of cross-bridges (Brutsaert and Sys 1989).

The results are given as mean value  $\pm$ SEM together with the results of the statistical proof by the Wilcoxon test for independent samples at  $p \pm 0.05$ .

#### *Scheme for cross-bridge cycling*

The following scheme (Yue 1987), describing 4 states (S1..S4) of the cross-bridge cycle, was used to relate the effects of BDM on the isometric mechanogram to alterations of cross-bridge kinetics. To quantify these suggested alterations, we employed a mathematical model based on the scheme (see the appendix).



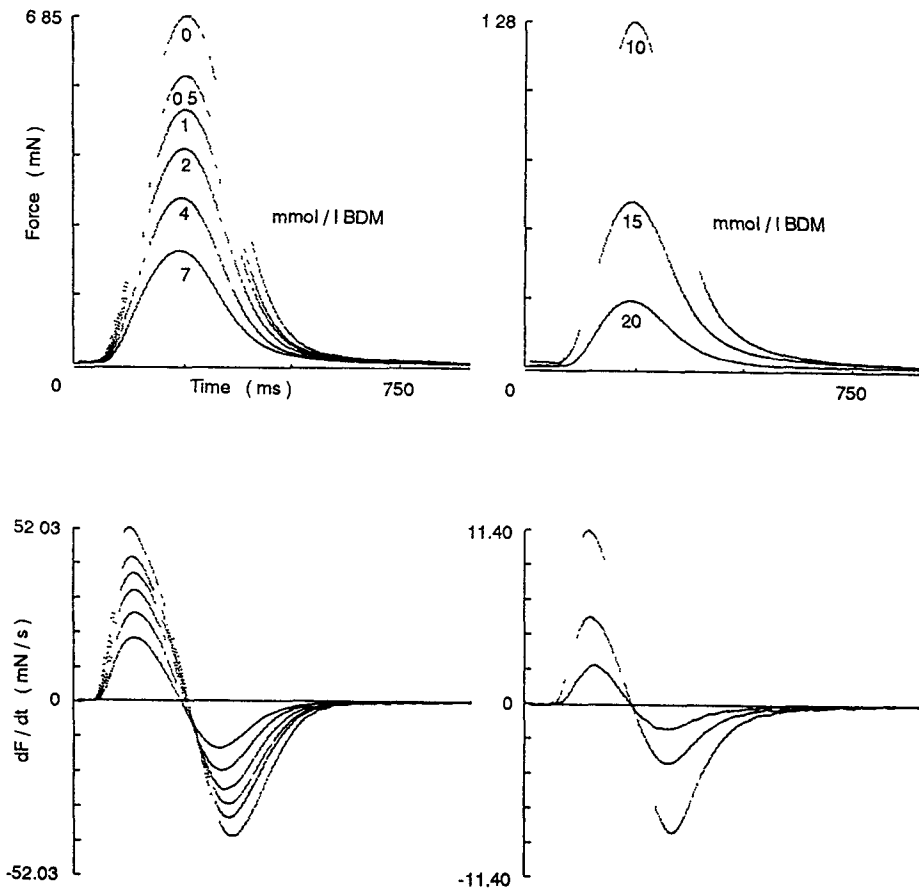
Force  $F$  is assumed to be proportional to the instantaneously existing number of myosin- (M) actin- (A) troponin- (T) complexes in S3 and S4, i.e.  $F \sim [\text{Ca-TA-M}] + [\text{TA-M}]$ .

At the resting level of  $\text{Ca}_i$ , A and M are separated in S1. Synchronously with increasing  $\text{Ca}_i$ , Ca binds to T (Housmans 1991; Peterson et al. 1991), because the high values for  $k_1$  and  $k_{-1}$  lead rapidly to an equilibrium between S1 and S2. S2 dominates because of  $k_1 \gg k_{-1}$ . Ca-TA is a prerequisite for the binding of M to A and for the delayed transition into the force producing state S3, corresponding to a low value of  $f$ . The constant  $g'$  is so low that the reverse reaction is virtually impossible (Yue 1987). Thus, the transition S2→S3 also occurs at low  $\text{Ca}_i$  and low  $[\text{Ca-TA}]$  at low rate. The instantaneous value of  $dF/dt$  is the difference between the rate of cross-bridge attachment, expressed by  $dF/dt_+$ , and detachment, expressed by  $dF/dt_-$ . It follows:

$$\begin{aligned}
 dF/dt &= dF/dt_+ - dF/dt_- \sim \frac{d[\text{Ca-TA-M}]}{dt} + \frac{d[\text{TA-M}]}{dt} \\
 dF/dt_+ &\sim \frac{k_1}{k_{-1}} f [\text{Ca}] [\text{TA}]
 \end{aligned} \tag{1}$$

The detachment of active cross-bridges requires dissociation of Ca from TnC (S4). S3 is favoured in the equilibrium between S3 and S4 by the high affinity of TnC for Ca ( $k_2 \gg k_{-2}$ ). Therefore, the dissociation of Ca from TnC is only possible at very low  $\text{Ca}_i$ . The decline of the number of active cross-bridges is expressed by:

$$dF/dt_- \sim \frac{k_{-2}}{k_2} g [\text{Ca-TA-M}] \tag{2}$$



**Figure 1.** Typical negative inotropic effect of increasing BDM concentrations on the isometric mechanogram of guinea-pig papillary muscle at 18 mmol/l extracellular Ca (experiment MBD 10).

The value  $dF/dt_{\max}$  should mainly be determined by  $dF/dt_+$  when the detachment rate is still negligible, and analogous  $dF/dt_{\min}$  by  $dF/dt_-$  when the attachment rate is expected to be already very low.  $PF$  is reached when the rates of attachment and detachment of cross-bridges become equal.

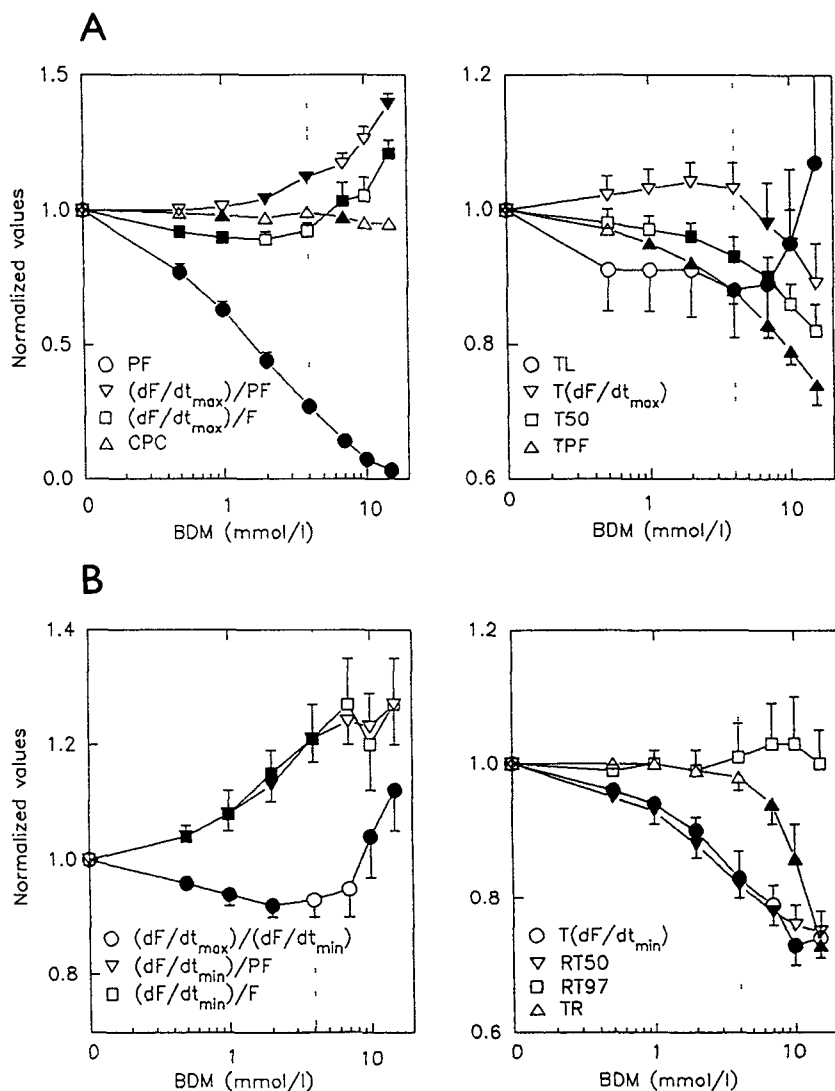
## Results

In papillary muscles  $PF$  reached a mean value of 7.8 mN at 18 mmol/l  $Ca_e$ . The cumulative addition of BDM produced a clear concentration-dependent negative inotropic effect (Fig. 1). The amplitude of twitch was more influenced than its time course.

Relative changes of isometric twitch parameters produced by BDM are shown in Fig. 2. Up to 4 mmol/l BDM,  $T(dF/dt_{\max})$ ,  $TL$  and  $CPC$  remained nearly constant. BDM shortened  $TPF$  mainly at the cost of  $TPF - T50$ . The increase in  $(dF/dt_{\max})/PF$  demonstrated a more prominent decrease of  $PF$  compared with  $dF/dt_{\max}$ , whereas  $(dF/dt_{\max})/F$  remained unchanged.

$T(dF/dt_{\min})$  and  $RT50$ , representing the early relaxation, were shortened. Together with the late phase of contraction, this resulted in the narrow peak of the twitch (Figs. 1 and 3).

$RT97$  was hardly influenced. The decrease of  $PF$  and of corresponding instan-



taneous  $F$  was greater than that of  $dF/dt_{\min}$ , resulting in a similar enhancement of  $(dF/dt_{\min})/PF$  and  $(dF/dt_{\min})/F$ .

At BDM concentrations exceeding 4 mmol/l additional effects appeared. The mechanical refractory period  $TR$ , i.e. the shortest stimulus interval eliciting a new contraction, was diminished.

Concerning the contraction,  $(dF/dt_{\max})/F$  and  $TL$  were increased, whereas  $T(dF/dt_{\max})$  and  $CPC$  were decreased.

Concerning the relaxation,  $(dF/dt_{\min})/PF$ ,  $(dF/dt_{\min})/F$ ,  $T(dF/dt_{\min})$ ,  $RT50$  and  $CPR$  remained relatively constant. After a decrease at low BDM concentration,  $(dF/dt_{\max})/(dF/dt_{\min})$  rose with increasing [BDM].

In isolated cardiomyocytes 4 mmol/l BDM depressed cellular contraction by about 80% (Fig. 4), i.e. to a similar extent as  $PF$  in papillary muscle (Fig. 1). The amplitude and the time course of the Ca transients (Fig. 4) as indices of the change in  $Ca_i$  were less affected as reported by others (Marijic et al. 1991; Gambassi et al. 1993).

The rate constants  $f$  for attachment and  $g$  for detachment of cross-bridges were estimated by a fitting procedure (see the appendix) from 9 mechanograms of

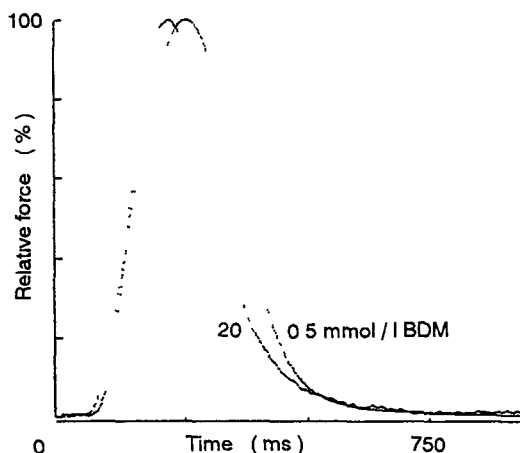
**Figure 2.** Mean normalized values and standard errors of parameters for the time courses of contraction (A) and relaxation (B) of guinea-pig papillary muscle at 18 mmol/l extracellular Ca as influenced by rising concentration of BDM;  $n = 10$ . Statistical significance versus the preceding value is marked by filled symbols.  $CPR$  is not shown in the figure because of its close correspondence to  $(dF/dt_{\min})/PF$  at constant  $RT97$ . Absolute values of parameters for the time courses of contraction (A) and relaxation (B) at 18 mmol/l extracellular Ca before the addition of BDM serving as control (corresponding to 1 as normalized values).

A

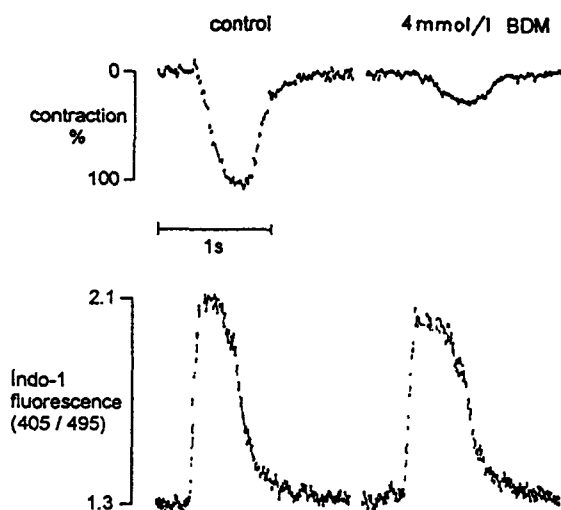
|           | $PF$ | $dF/dt_{\max}$ | $\frac{dF/dt_{\max}}{PF}$ | $\frac{dF/dt_{\max}}{F}$ | $TL$ | $T(dF/dt_{\max})$ | $T50$ | $TPF$ | $CPC$ |
|-----------|------|----------------|---------------------------|--------------------------|------|-------------------|-------|-------|-------|
|           | mN   | mN/s           | 1/s                       | 1/s                      | ms   | ms                | ms    | ms    |       |
| mean      | 7.84 | 61.73          | 7.89                      | 20.63                    | 38.8 | 110.4             | 125.2 | 240.4 | 1.59  |
| $\pm$ SEM | 0.95 | 7.65           | 0.14                      | 0.60                     | 4.1  | 5.4               | 4.5   | 4.6   | 0.01  |

B

|           | $dF/dt_{\min}$ | $\frac{dF/dt_{\max}}{dF/dt_{\min}}$ | $\frac{dF/dt_{\min}}{PF}$ | $\frac{dF/dt_{\min}}{F}$ | $T(dF/dt_{\min})$ | $RT50$ | $RT97$ | $CPR$ | $TR$  |
|-----------|----------------|-------------------------------------|---------------------------|--------------------------|-------------------|--------|--------|-------|-------|
|           | mN/s           |                                     | 1/s                       | 1/s                      | ms                | ms     | ms     |       | ms    |
| mean      | 43.68          | 1.40                                | 5.69                      | 8.91                     | 98.8              | 125.4  | 289.8  | 1.64  | 243.0 |
| $\pm$ SEM | 4.78           | 0.05                                | 0.22                      | 0.47                     | 3.4               | 3.5    | 7.3    | 0.03  | 5.6   |



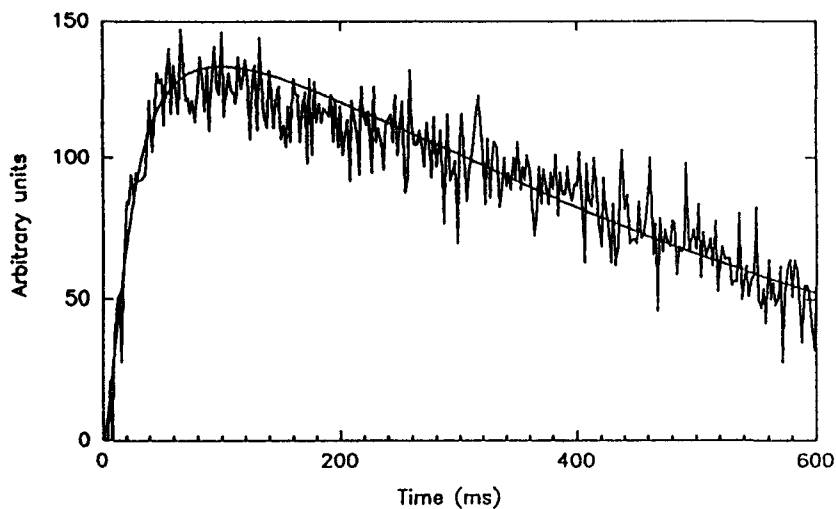
**Figure 3.** Comparison of the normalized mechanograms of guinea-pig papillary muscle at 0.5 and 20 mmol/l BDM (experiment MBD 10)



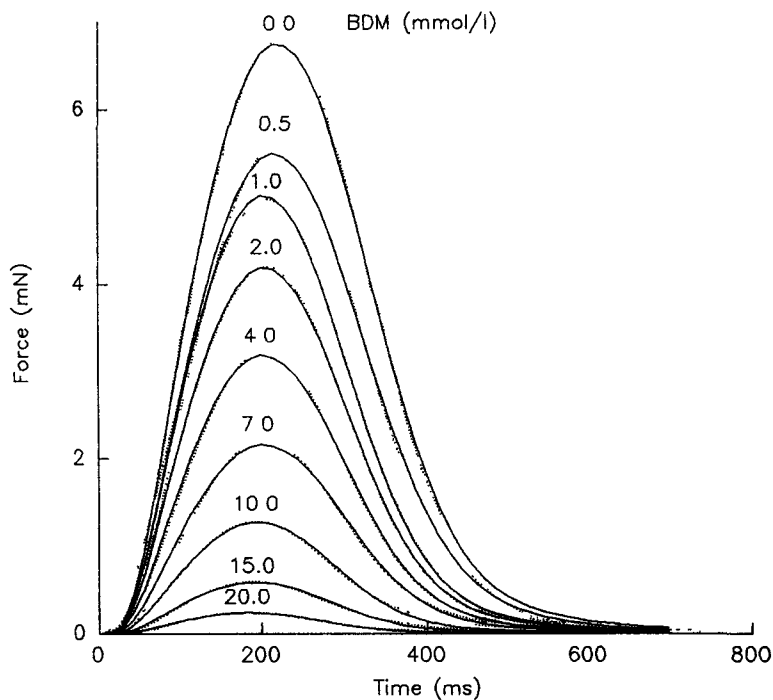
**Figure 4.** Example of a Ca transient and contraction of isolated guinea-pig cardiomyocyte at 0 (control) and 4 mmol/l BDM. Under these conditions the contraction amplitude was reduced to  $20.2 \pm 1.8\%$ , whereas the nearly unchanged Ca transient reached an amplitude of  $106.1 \pm 3.6\%$  (mean values  $\pm$  SEM compared to control = 100%;  $n = 6$ ).

a typical experiment recorded at rising concentrations of BDM from 0 up to 20 mmol/l. These mechanograms were combined with a physiological Ca transient measured in isolated guinea-pig cardiomyocytes in the absence of BDM (Fig. 5) which fulfils two important characteristics for the fitting procedure, e.g. the coincidence between peak  $Ca_i$  ( $Ca_{i,max}$ ) and  $T(dF/dt_{max})$  (Yue 1987) and the slow decline of  $Ca_i$ . This approach based on the cross-bridge scheme yielded fitted curves in close conformity with the original signals (Fig. 6). Low BDM induced a decrease of  $f$  and an increase of  $g$  to a similar extent, leading to a clear decrease of their ratio (Fig. 7).

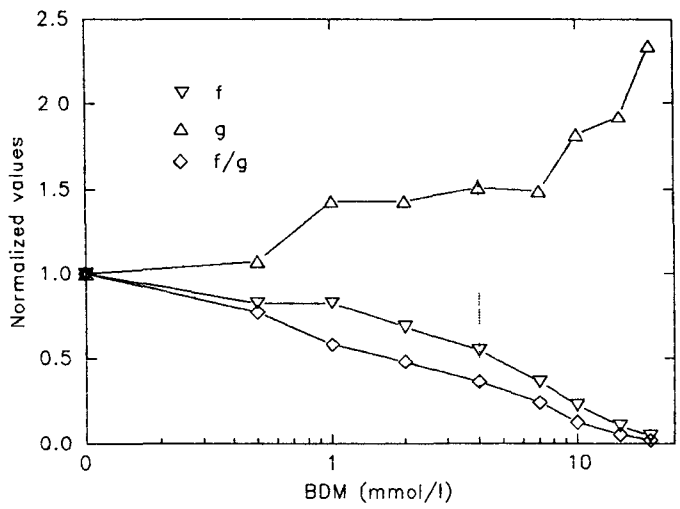




**Figure 5.** Intracellular calcium under normal conditions (no BDM). The experimental data were fitted to the phenomenological expression (6) (see appendix).



**Figure 6.** Mechanograms recorded at various concentrations of BDM (dotted line) and fitted solutions of differential equation (5) (solid line) (see appendix).



**Figure 7.** Change of the rate constants  $f$  and  $g$  at increasing concentrations of BDM. Plot of the relative rate constants  $f$  and  $g$  (normalized to their values without BDM). There is a monotonous decline of the rate constant  $f$ , whereas the rate constant  $g$  after abrupt increase at low concentration of BDM remains practically constant for BDM concentrations of up to 8 mmol/l. The absolute values are:

|              |      |      |      |      |      |       |       |       |       |
|--------------|------|------|------|------|------|-------|-------|-------|-------|
| BDM (mmol/l) | 0.0  | 0.5  | 1.0  | 2.0  | 4.0  | 7.0   | 10.0  | 15.0  | 20.0  |
| $f$ (1/s)    | 3.5  | 2.9  | 2.9  | 2.4  | 1.9  | 1.25  | 0.79  | 0.37  | 0.16  |
| $g$ (1/s)    | 25.2 | 27.0 | 36.0 | 36.0 | 38.0 | 37.50 | 45.70 | 48.40 | 59.00 |

Discussion

Suppression of  $PF$  and modifications of the mechanogram observed at low concentrations of BDM (up to 4 mmol/l) are regarded to be related to its effects on the  $Ca$  sensitivity of the myofilaments, because within this range the  $Ca_i$  transient was not reduced in papillary muscle of the guinea-pig (Marijic et al.1991) as confirmed by our experiments in isolated cardiomyocytes.

An assumed decrease in the affinity of TnC for  $Ca$  (Gwathmey and Solaro 1990; Wang and Lee 1990; Marijic et al. 1991) was not confirmed by direct measurement of  $Ca$  binding to TnC under BDM in heart (Mulieri and Alpert 1984; Gwathmey et al. 1991) and skeletal muscle (Fuchs and Wang 1991). Therefore, other components involved in the cross-bridge kinetics are most probably responsible (Li et al. 1985; Higuchi and Takemori 1989; West and Stephenson 1989; Kurihara et al. 1990; Dantzig et al. 1991; Herrmann et al. 1992; Perreault et al. 1992; Gambassi et al. 1993; Venema et al. 1993; Backx et al. 1994; Zhao and Kawai 1994).

### Contraction

$T(dF/dt_{\max})$  reflects the moment of  $Ca_i$ max (Yue 1987; Housmans 1991; Peterson et al. 1991), because maximum  $[Ca_i]$  produces maximum  $dF/dt_+$ , i.e.  $dF/dt_{\max}$  (cf. equation 1). Therefore, the constant value of  $T(dF/dt_{\max})$  at BDM concentrations of up to 4 mmol/l is well in agreement with a less influenced  $Ca_i$  transient measured in isolated cardiomyocytes. The unchanged value of  $CPC$  means that at low BDM concentration the sources of Ca are not significantly influenced.

Assuming a reduced Ca sensitivity of myofilaments under BDM, a higher  $Ca_i$  would be required to reach the mechanical threshold, accompanied by prolonged  $TL$ , which is indeed measurable at high BDM concentrations.

At low Ca sensitivity, expressed by low ratio of  $f$  and  $g$ , the fall in  $Ca_i$  after  $T(dF/dt_{\max})$  and  $Ca_i$ max, respectively. (Yue 1987; Housmans 1991; Peterson et al. 1991) decelerates further increase in force. When the diminished rate of cross-bridge attachment is exceeded by the rising rate of detachment,  $PF$  will be reached earlier. Thus, points of time following  $T(dF/dt_{\max})$ , like  $T50$  and  $TPF$ , are shifted towards  $T(dF/dt_{\max})$ , as especially seen for the interval between  $T50$  and  $TPF$ .

Both the earlier termination of the increase in force and the lower  $dF/dt_+$  are responsible for the strong negative inotropic effect of BDM, as seen by the discrepancy between  $(dF/dt_{\max})/F$  and  $(dF/dt_{\max})/PF$ . The reduced rate constant  $f$  causes a slower transition into force generating states, followed by a decline of  $dF/dt_+$  (equation 1). Then  $dF/dt_{\max}$  and  $F$  are reduced in proportion after an identical  $T(dF/dt_{\max})$ . Consequently,  $(dF/dt_{\max})/F$  remains nearly constant.

The stronger decrease in  $PF$  compared to  $dF/dt_{\max}$  increases  $(dF/dt_{\max})/PF$ . The constant value of  $CPC$ , defined as  $CPC = (dF/dt_{\max})/PF \cdot (TPF - TL)$ , means that the increase in  $(dF/dt_{\max})/PF$  is compensated by the decrease in  $(TPF - TL)$ . The same is seen in the normalized curves under high BDM (Fig. 3), where, after a prolonged  $TL$ , the peak force is reached earlier, i.e.  $dF/dt$  remains relatively greater. Therefore, the earlier termination of the increase in  $F$  and the lower  $dF/dt$  interact synergistically.

In the early termination of the increase in force, two processes are involved. The BDM dependent decline of  $f$  reduces the rate of the formation of active cross-bridges (equation 1). Otherwise, the increase in  $g$  indicates a higher rate of the dissociation of active cross-bridges (equation 2). Thus, the formation and dissociation of cross-bridges become already equal at higher  $Ca_i$ . The shift of contraction to relaxation appears therefore earlier, at unchanged  $Ca_i$ .

### Relaxation

The decreases in  $T(dF/dt_{\min})$  and  $RT50$  demonstrate the short duration of the early relaxation.  $dF/dt_{\min}$  is reached when  $F$  is  $0.66 \cdot PF$ , given by  $F/PF = 0.66$  with a correlation coefficient of  $r = 0.99$ . Obviously,  $F$  and  $PF$  are influenced in the same manner by the lowered Ca sensitivity of myofilaments.

The shortening of  $T(dF/dt_{\min})$  is linearly related to the increases in  $(dF/dt_{\min})/PF$  and  $(dF/dt_{\min})/F$  ( $r = 0.7$ ). The lower diminishing of  $dF/dt_{\min}$  compared with  $PF$  and  $F$  leads to a faster decrease in force to  $F = 0.66 \cdot PF$  at  $T(dF/dt_{\min})$ . Consequently,  $F$  corresponds to a relatively higher  $dF/dt_{\min}$  under BDM, and the percentage of active cross-bridges detaching per time grows.

During relaxation, the decline of  $Ca_i$  proceeds and, as seen in the reaction scheme, the formation of cross-bridges becomes more and more negligible. Relaxation then mainly depends on the detachment of the existing cross-bridges. The increase in  $(dF/dt_{\min})/F$  with increasing BDM concentrations means that, related to the corresponding  $F$  (e.g. normalized to the number of active cross-bridges at  $0.66 \cdot PF$ ), the rate of cross-bridge detachment grows. This is possible, if the rate constant  $g$  is elevated (equation 2). Therefore,  $dF/dt_-$  is enhanced synergistically to a diminishing of  $dF/dt_+$  by BDM.

Comparing the maximum rates of formation and detachment of cross-bridges, low BDM diminishes  $dF/dt_{\max}$  more than  $dF/dt_{\min}$ , as seen by the decrease in  $(dF/dt_{\max})/(dF/dt_{\min})$ . This also indicates a reduced ratio of  $f$  and  $g$ .

#### *High BDM concentration*

At BDM concentrations exceeding 4 mmol/l, most of the twitch parameters are markedly influenced. The shortening of  $T(dF/dt_{\max})$  suggests a shortening of the time to peak of  $Ca_i$  (Yue 1987). The shorter  $T(dF/dt_{\max})$  is explained by a probably reduced  $Ca_i$  supply (Li et al. 1985; Horiutu et al. 1988; Chapman 1993; Liu et al. 1993; Steele and Smith 1993) at shorter action potential duration (Chapman 1993; Liu et al. 1993) together with an earlier onset of removal of  $Ca$  from the cytosol brought about by the  $Ca$  outward transport via  $Na/Ca$  exchange (Brutsaert and Sys 1989). In the guinea-pig myocardium, release and reuptake of  $Ca$  by the SR is less developed (Horackova 1989) and additionally inhibited by high BDM in myocardium (Steele and Smith 1993). On the other hand, the  $Na/Ca$  exchange is the main mechanism for the removal of  $Ca_i$  (Horackova 1989). Therefore, influences on its driving force are expected to become visible in the mechanogram. A shortening of the action potential by high BDM concentrations (Li et al. 1985; Chapman 1993; Liu et al. 1993) is in agreement with the significant shortening of the mechanical refractory period  $TR$ . Thereby the reversal of  $Ca$  entry to  $Ca$  outward transport starts earlier, followed by an earlier peak of  $Ca_i$  and an earlier onset of its decline.

Under high BDM concentrations the formation and detachment of cross-bridges, due to the lowered ratio of  $f$  and  $g$ , was modified by a diminished but long lasting  $Ca$  transient (Blanchard et al. 1990; Perreault et al. 1992; Spurgeon et al. 1992; Gambassi et al. 1993; Kotsanas et al. 1993). Relaxation rate decreases now in proportion to  $PF$  without significant shortening of time. So  $dF/dt_{\max}$  is less reduced than  $dF/dt_{\min}$ , resulting in increased  $(dF/dt_{\max})/(dF/dt_{\min})$ . The

tonic and phasic components of contraction are less sharply separated, as seen by the decline of *CPC*. Especially the very early onset and the fast decline of *F* is responsible for the continuous increase in *CPR*.

In conclusion, the results showed how the cellular mechanism(s) of the BDM induced negative inotropic effect, i.e. mainly the lowered ratio of rate constants for cross-bridge attachment and detachment, leads to a characteristic modification of the isometric mechanogram. The reaction scheme (Yue 1987) for the formation and detachment of cross-bridges is a suitable tool to explain the causal connection between the cellular effect and the modified mechanogram.

## Appendix

The kinetic equations related to the scheme of the cross-bridge cycle (see above) read

$$\begin{aligned}\frac{d}{dt} [\text{TA}] &= g [\text{TA-M}] - k_1 [\text{Ca}]^n [\text{TA}] + k_{-1} [\text{Ca-TA}] \\ \frac{d}{dt} [\text{Ca-TA}] &= k_1 [\text{Ca}]^n [\text{TA}] - (k_{-1} + f) [\text{Ca-TA}] \\ \frac{d}{dt} [\text{Ca-TA-M}] &= f [\text{Ca-TA}] - k_{-2} [\text{Ca-TA-M}] + k_2 [\text{Ca}]^n [\text{TA-M}] \\ \frac{d}{dt} [\text{TA-M}] &= k_{-2} [\text{Ca-TA-M}] - (k_2 + g) [\text{TA-M}]\end{aligned}\quad (1)$$

Under the assumption

$$k_1, k_{-1}, k_2, k_{-2} \gg f, g \quad (2)$$

equation system (1) can be simplified by means of the quasi-steady-state approximation (Schauer and Heinrich 1983) describing the binding of calcium to [TA] and [TA-M] by mass-action relations,

$$\frac{[\text{Ca-TA}]}{[\text{Ca}]^n [\text{TA}]} = \frac{k_1}{k_{-1}} = \Gamma_1; \quad \frac{[\text{Ca-TA-M}]}{[\text{Ca}]^n [\text{TA-M}]} = \frac{k_2}{k_{-2}} = \Gamma_2 \quad (3)$$

Introducing new variables  $[X_1] = [\text{TA}] + [\text{Ca-TA}]$  and  $[X_2] = [\text{TA-M}] + [\text{Ca-TA-M}]$  which fulfil the conservation condition  $[X_1] + [X_2] = \text{const} = [X]$  and taking into account the relations (3) we arrive at the following differential equation for the variable  $[X_2]$ ,

$$\frac{d}{dt} [X_2] = f \frac{\Gamma_1 [\text{Ca}]^n}{1 + \Gamma_1 [\text{Ca}]^n} ([X] - [X_2]) - g \frac{[X_2]}{1 + \Gamma_2 [\text{Ca}]^n} \quad (4)$$

The contractile force is assumed to be proportional to  $[X_2]$ , i.e.  $F = \gamma [X_2]$ , so that equation (4) can be easily transformed into a differential equation for  $F$ ,

$$\frac{d}{dt} F = F_0 \frac{f}{1 + \left(\frac{K_1}{[\text{Ca}]}\right)^n} - \left( \frac{f}{1 + \left(\frac{K_1}{[\text{Ca}]}\right)^n} + \frac{g}{1 + \left(\frac{[\text{Ca}]}{K_2}\right)^n} \right) F \quad (5)$$

where  $F_0 = \gamma[X]$  and  $K_i = 1/\Gamma_i^{1/n}$ . In order to solve this equation one needs to know the time dependent intracellular calcium concentration  $[Ca]$ . We employed the phenomenological expression

$$[Ca] = \frac{[Ca]_0}{\left(1 + \left(\frac{T_0}{t}\right)^{n_c}\right) (1 + \exp(a[t - T_0]))} \quad (6)$$

for  $[Ca]$  which was fitted to experimental data. Estimated parameters are:  $Ca_0 = 332.4$  (Ca-units),  $T_0 = 25.1$  ms,  $n_c = 1.6$ ,  $a = 0.0029$  1/ms. The introduction of expression (6) with these estimated parameter values into equation (5) results in a single differential equation for  $F$  which contains the unknown parameters  $f$ ,  $g$ ,  $K_1$ ,  $K_2$ ,  $n$  and  $F_0$ . Recent findings (Li et al. 1985; Higuchi and Takemori 1989; Fuchs and Wang 1991; Perreault et al. 1992; Gambassi et al. 1993; Khandoudi et al. 1993; Venema et al. 1993; Backx et al. 1994) suggest that BDM influences mainly the rate constants  $f$  and  $g$ , whereas the half-saturation constants  $K_1$ ,  $K_2$ , the cooperativity index  $n$  for calcium binding and the maximal force  $F_0$  are assumed to remain unaltered. Thus there were  $4 + 2 \times 8 = 20$  adjustable parameters to be estimated by fitting the numerical solutions of differential equation (5) simultaneously to 9 different isometric mechanograms recorded at varying concentrations of BDM between 0 and 20 mmol/l. The fit was performed by using the software package "SIMFIT" (Holzhütter and Colosimo 1990). The estimated parameter values are:  $K_1 = 199.4$  (Ca-units),  $K_2 = 99.7$  (Ca-units),  $n = 3.8$ ,  $F_0 = 101$  mN, rate constants  $f$  and  $g$  cf. absolute values in legend to Fig. 7.

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